Aggrecan: Resists Compression (in tissues) Collagen: Resists Tension (in tissues)



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~Equilibrium

Stress vs strain curve of
 rat tail tendon:
(A-B) "Toe" region,
(C) ~linear region (~HILE)
(D) plateau,
(E) rupture of the tendon.

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- Need 2 independent measurements (2 moduli), to completely characterize an elastic tissue
- Every elastic modulus can then be expressed in terms of those 2 moduli

	bulk	Young's	Lamé #2	Shear	Poisson	Longitudinal
	(K =)	E =	$\lambda =$	G =	$\nu =$	$M = \mathbf{H}$
(K, E)	K	E	$\tfrac{3K(3K-E)}{9K-E}$	$\frac{3KE}{9K-E}$	$\frac{3K-E}{6K}$	$\tfrac{3K(3K+E)}{9K-E}$
(K, λ)	K	$\frac{9K(K-\lambda)}{3K-\lambda}$	λ	$\frac{3(K-\lambda)}{2}$	$\frac{\lambda}{3K-\lambda}$	$3K-2\lambda$
(K, G)	K	$\frac{9KG}{3K+G}$	$K - \frac{2G}{3}$	G	$\frac{3K-2G}{2(3K+G)}$	$K + \frac{4G}{3}$
(K, ν)	K	$3K(1-2\nu)$	$\frac{3K\nu}{1+\nu}$	$\tfrac{3K(1\!-\!2\nu)}{2(1\!+\!\nu)}$	ν	$\frac{3K(1-\nu)}{1+\nu}$
(K, M)	K	$\frac{9K(M-K)}{3K+M}$	$\frac{3K-M}{2}$	$\frac{3(M-K)}{4}$	$\frac{3K-M}{3K+M}$	M
(E, λ)	$\frac{E+3\lambda+R}{6}$	E	λ	$\frac{E-3\lambda+R}{4}$	$\frac{2\lambda}{E+\lambda+R}$	$\frac{E-\lambda+R}{2}$
(E, G)	$\frac{EG}{3(3G-E)}$	E	$\frac{G(E{-}2G)}{3G{-}E}$	G	$\frac{E}{2G} - 1$	$\frac{G(4G-E)}{3G-E}$
(E, ν)	$\frac{E}{3(1-2\nu)}$	E	$\frac{E\nu}{(1+\nu)(1-2\nu)}$	$\left(\frac{E}{2(1+\nu)}\right)$	ν	$\frac{E(1-\nu)}{(1+\nu)(1-2\nu)}$
(λ, G)	$\lambda + \frac{2G}{3}$	$\underbrace{\frac{G(3\lambda+2G)}{\lambda+G}}$	λ	G	$\frac{\lambda}{2(\lambda+G)}$	$\lambda + 2G$

Regulation of gene expression in intervertebral disc cells by low and high hydrostatic pressure

(Eur Spine J, 2006)

Cornelia Neidlinger-Wilke · Karin Würtz · Jill P. G. Urban · Wolfgang Börm · Markus Arand · Anita Ignatius · Hans-Joachim Wilke · Lutz E. Claes



hydraulic load frame (Instron)

Fig. 1 Scheme of the stimulation device for the application of high hydrostatic pressure (2.5 MPa) and photo of a sterile bag with cell-seeded collagen gels

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Intervertebral Disc

(Peter Roughley, Spine, 2004)



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"Creep-Compression" of intervertebral disc (rat tail)



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(MacLean+, J Biomechanics, 2007)

"Creep-Compression" of intervertebral disc (rat tail):

Apply constant stress (σ_{11}) and measure displacement (strain) vs time



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(MacLean+, J Biomechanics, 2007)

Influence of Decorin and Biglycan on Mechanical Properties of Multiple Tendons in Knockout Mice



Apply step in strain (ϵ_{11}) and <u>measure stress vs time</u>

Mouse tendon fascicle



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Robinson+, J Biomech Eng, 2005

Influence of Decorin and Biglycan on Mechanical Properties of Multiple Tendons in Knockout Mice



Apply step in strain (ϵ_{11}) and <u>measure stress vs time</u>

Mouse tendon fascicle





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 rat tail tendon:
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"Stress Relaxation"

Molecular- & Tissue-level Mechanisms??

Mouse tendon fascicle



Tendon Hierarchy Evidence : x ray x ray x ray EΜ SEM FM ĒΜ SEM ΕM OM SEM OM x ray Tissue TENDON FASCICLE TROPO-COLLAGEN 35 Å staining 640 Å periodicity sites Molecule reticular Fibri waveform membrane fibroblasts fascicular s or crimp structure membrane 15Å 35Å 100-200 Å 500-5000 Å 50-300 µ 100-500 u SIZE SCALE

Figure 7.3:6 Hierarchy of structure of a tendon according to Kastelic et al. (1978). Reproduced by permission. Evidences are gathered from X ray, electron microscopy (EM), scanning electron microscopy (SEM), and optical microscopy (OM). (Y.C. Fung)

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PROTEOGLYCAN SUPERFAMILY

• ECM molecules with (1) Core protein, and (2) Glycosaminoglycan (GAG) chains

- "Sub-families" include
 - <u>Extracellular</u> Large Aggregating (Aggrecan)
 <u>Small Leucine-Rich PG</u> (SLRPs)

- <u>Cell Surface</u> (e.g., glycocalyx HSPGs)

Proteoglycans

Encyclop Life Sci, 2009

Nancy B Schwartz, University of Chicago, Illinois, USA



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Decorin & Collagen Fibrillogenesis



Courtesy of The Journal of Biological Chemistry. Used with permission. Source: Iozzo, Renato V. "The Biology of the Small Leucine-rich Proteoglycans Functional Network of Interactive Proteins." *Journal of Biological Chemistry* 274, no. 27 (1999): 18843-6.





SKIN decorin KO

decorin KO

Normal (WT)

Example of Small-Leucine-Rich Proteoglycans

Figure 4 Ultrastructural appearance of dermal collagen from the skin of decorin null (A and B) and wild-type (C) mice. Notice the larger and irregular cross-sectional profiles in the decorin null collagen fibers (*asterisks*) with evidence of lateral fusion (A, *arrowheads*). Bar: 90 nm.

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(lozzo +, Normal and decorin null mice, J Biol Chem 1999)



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Gauteri, Buehler et al., Matrix Biology, 31:141-9, 2012

Influence of Decorin and Biglycan on Mechanical Properties of Multiple Tendons in Knockout Mice



Apply step in strain (ϵ_{11}) and measure stress vs time



Patellar (left) and flexor digitorum longus (right)

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"Lumped Element" Viscoelastic Models Viscoelastic properties of model segments of collagen molecules Alfonso Gautieri ^{a, b}, Simone Vesentini ^b, Alberto Redaelli ^b, Markus J. Buehler ^{a, c,*}

-a deep understanding of the relationship between molecular structure and mechanical properties remains elusive, hindered by the complex hierarchical structure of collagen-based tissues...
- Although extensive studies of viscoelastic properties have been pursued at the macroscopic (fiber/tissue) level, fewer investigations have been performed at the smaller scales, including collagen molecules and fibrils.
- Here, using atomistic modeling, we perform <u>"in silico" creep tests</u> of a collagen-like peptide.....<u>relate time-dependence to molecular</u> <u>structure</u>



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"In silico" creep test of a segment of a collagen molecule



Fig. 1. Snapshots of the collagen peptide in water box. Panel a shows the conformation of the full atomistic model of a $[(GPO)_{21}]_3$ collagen peptide solvated in water box and equilibrated for 30 ns. After equilibration the molecule is subjected to virtual creep tests: one end of the collagen peptide is held fixed, whereas the other end is pulled with constant force (from 300 pN to 3000 pN) until end-to-end distance reaches equilibrium (Panel b). Panel c shows a schematic of the creep test; a constant force is applied instantaneously to the molecule and its response (deformation over time) is monitored. The mechanical response of collagen molecule is modeled using a KV model, from which molecular Young's modulus (*E*) and viscosity (η) are calculated.

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Fig. 2. Single molecule creep test. Mechanical response of solvated collagen molecule to creep tests for three cases with increasing value of external force. Dots represent the experimental data, whereas curves represent the fitted curves using a Kelvin–Voigt model.

τ = (η/E) ~ 0.5 ns



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to stretching. On the other hand, the viscous behavior may be due to the breaking and reforming of H-bonds, in particular H-bonds between the three collagen chains.

"In silico" creep test of a segment of a collagen molecule



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Robinson+, J Biomech Eng, 2005



the viscous behavior of fibrils and fibers involves additional mechanisms, such as molecular sliding between collagen molecules within the fibril <u>or effects of relaxation of larger volumes of solvent</u>

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